

Time-Frequency Analysis of 24-Hour Heart Rate Fluctuation for the Characterization of Very Low-Frequency Component

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Abstract - A smooth pseudo Wigner-Ville distribution was employed to investigate both time and frequency characteristics in very low-frequency component (less than 0.04 Hz) of 24-hour heart rate fluctuation. In some of heart failure, we could see remarkable and very low-frequency oscillations on the Wigner-Ville distribution, which are related to Cheyne-Stokes respiration. However, the Wigner-Ville distribution of normal subjects had not such oscillations, but more random spectral characteristics instead. Furthermore, we calculated $1/f^\alpha$ regression slopes of average spectrum to be a crude estimate of fractal dimensions. The slopes are more negative in heart failure than normal (-1.866 ± 0.888 vs. -0.957 ± 0.180 $p < 0.005$), which associates a loss of dimensionality of heart rate fluctuation in heart failure.

INTRODUCTION

Spectral analysis of heart rate variability provides a way to understand the different control mechanisms of the autonomic nervous system. In previous researches[1], the high frequency fluctuations of heart rate (approximately 0.15-0.40 Hz) were regarded as vagal control, and were correlated with respiration. And, the low frequency fluctuations (approximately 0.04-0.15 Hz) were due to both sympathetic and vagal control. However, for the implicated mechanism of very low-frequency fluctuations (less than 0.04 Hz), there were some hypothesis and observations, such as renin-angiotension regulation [1], temperature regulation [2], a chaotic behavior[3], and a long-wavelength oscillation in heart failure[4]. In clinical study, power in very low-frequency band differentiated the heart failure group from the normal group[5]. Moreover, it had strong association with mortality after myocardial infarction[6]. Thus, we regarded it might imply some physiological or pathological information in very low-frequency heart rate.

One problem exists in the analysis of very-low frequency heart rate : what is the proper size of time window for spectral analysis? A particular window should be appropriate for a particular signal to give better frequency resolution. Longer window could provide better frequency resolution, but would smear the time-varying characteristic of signals (*ie*, poor time resolution). To overcome this problem, we employed Wigner-Ville distribution to reveal possible phenomenon in very low-frequency band of 24-hour heart rate.

METHODS

A. Subjects and preliminary processing

Thirteen heart failure patients and fourteen normal subjects were included for this study. All subjects underwent 24-hour Electrocardiogram recording. ECG signals were digitized into PC for QRS detection and verification. The instantaneous heart rate were equal-sampling (2 Hz) using cubic spline interpolation. In order to reduce the heavy computation in Wigner-Ville distribution, the sampling rate of heart rate was further reduced to 0.2 Hz. Before subsampling, original heart rate were filtered with a FIR low-pass filter with 0.08 Hz cut-off frequency to avoid aliasing.

B. Smooth pseudo Wigner-Ville distribution (SPWVD)

The SPWVD of a heart rate signal $s(n)$ is expressed as follows :

$$SPWVD(n, k) = \sum_{i=-N+1}^{N-1} |h(i)|^2 \left[\sum_{m=-M+1}^{M-1} g(m) z(n+m+i)z^*(n+m-i) \right] \exp(-j\frac{2\pi}{N}ik) \quad (1)$$

where $h(i)$ is a Gaussian window, $g(m)$ is a rectangular window, and $z(n)$ is the analytic signal associated with real heart rate signal $s(n)$. It is calculated in the time domain as follows :

$$z(n) = s(n) + jH[s(n)] \quad (2)$$

where $H[.]$ is Hilbert transform.

Using windows of $h(i)$ and $g(m)$, it allows independent smoothing in both directions, frequency and time, by selecting different window size, $2N - 1$ and $2M - 1$ respectively [7,8]. Also, it can reduce cross terms which may encounter in WVD. The use of the analytic signal could avoid low-frequency artifacts and aliasing components produced in the real Wigner distribution [9].

C. $1/f^\alpha$ regression slope

In order to study the fractal dimensions of heart rate fluctuation, the average spectrum, time integration of Wigner-Ville distribution, were characterized as an inverse power-law ($1/f^\alpha$ -like) spectrum within the following frequency band : the highest frequency was set to 0.04 Hz,

and the lowest frequency was the peak frequency associated maximum power below 0.04 Hz. With steeper slope α , the fractal dimension of heart rate fluctuation would be smaller, and vice versa.

RESULTS

Figure 1 shows the Wigner-Ville distribution of 24-hour heart rate fluctuation in a heart failure patient. One can easily see remarkable and very low-frequency oscillations during night, and more random spectrum in the other time. These oscillations are regarded as Cheyne-Stokes respiration (CSR)[3]. It implies that high degree freedom of heart rate fluctuation have become locked into a single wavelength during CSR. Meanwhile, the oscillation frequency, amplitude, duration, and occurrence time could be identified. However, the Wigner-Ville distribution of normal subjects have not such oscillations, but more random spectral characteristics instead.

Comparing regression slopes of average spectrum, we found it has statistical differences (-1.866 ± 0.888 vs. -0.957 ± 0.180 , $p < 0.005$). This result demonstrates that heart failure subjects yield more negative slopes than normal subjects, that is, it is associated with a loss of dimensionality of heart rate fluctuation in heart failure.

DISCUSSION

Very Low-frequency power of heart rate accounts most portion of total power in the spectrum of 24-hour heart rate. Unlike other higher frequency power, it is less directly related to the action of vagal or sympathetic system. By the transform of 24 heart rate to Wigner-Ville distribution, it not only provides more high-resolution spectral characteristics, but also reveals both frequency-varying and time-varying characteristics of signal. Therefore, it will be helpful for observing the very low-frequency dynamics of the regulation of the cardiovascular system.

Although there would exist cross terms in the Wigner-Ville distribution, these could be improved by appropriate selection of smoothing window ($g(m)&h(i)$) [8]. In addition, the computation work of this SPWVD is less heavy, compared with other interference-reduced WVD [9]. So it is suitable for signal with a large amount of data, such as 24 heart rate fluctuation signal.

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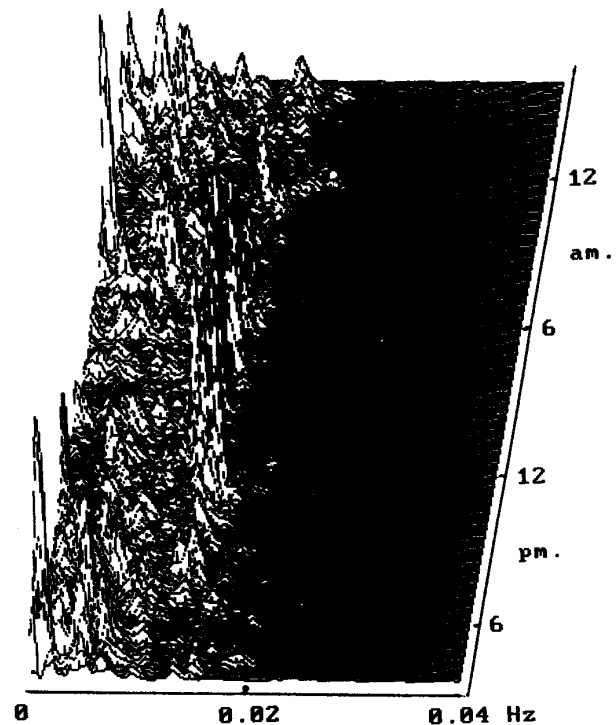


Figure 1: SPWVD of one heart failure patient. There are about 0.015 Hz low frequency oscillations during night, and are regarded as Cheyne-Stokes respiration.